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Cigarette smoking and airway wall thickness on CT scan in a multi-ethnic cohort: The MESA Lung Study

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Summary

Background: Autopsy studies show that smoking contributes to airway wall hyperplasia and narrowing of the airway lumen. Studies of smoking and airway measures on computed tomography (CT) scan are limited to case-control studies of measures that combine airway lumen and wall thickness.

Objectives: We hypothesized that cumulative cigarette smoking would be associated with increased airway wall thickness in a large, population-based cohort.

Methods: The Multi-Ethnic Study of Atherosclerosis enrolled participants age 45–84 years from the general population. Smoking history was assessed via standardized questionnaire items; current smoking was confirmed in half the cohort with cotinine. Airway lumen and wall thickness were measured in two dimensions in posterior basal segmental bronchi on cardiac-gated CT scans. Analyses were adjusted for age, gender, genetic ancestry, education, height, weight, asthma history, particulate matter, scanner type, and scanner current.

Results: Half of the 7898 participants had smoked and 14% were current smokers. Pack-years of smoking were associated with thicker airway walls (mean increase 0.002 mm per ten pack-years [95% CI: 0.00002, 0.004] $p = 0.03$). Current smoking was associated with narrower airway lumens (mean decrease -0.11 mm [95% CI: -0.2 , -0.02] $p = 0.02$). There was no evidence that either association was modified by genetic ancestry, and findings persisted among participants without clinical disease.

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Conclusions: Long-term cigarette smoking was associated with subclinical increases in wall thickness of sub-segmental airways whereas current smoking was associated with narrower airway lumen diameters. Smoking may contribute to airway wall thickening prior to the development of overt chronic obstructive pulmonary disease.

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Comments

This is the first large, population-based study of the relationship between smoking and airway dimensions on CT scan. We used a novel approach to assess separately the contributions of cumulative and current smoking on airway wall thickness and lumen diameter among $n = 7898$ participants in a multi-ethnic cohort. We found that cumulative cigarette smoking was associated with subclinical increases in sub-segmental airway wall thickness, whereas current cigarette smoking was associated with reduced lumen diameter. Smoking may contribute to chronic obstructive pulmonary disease chronically via airway wall thickening, and acutely via narrower lumens.

Introduction

Chronic lower respiratory disease is the third leading cause of death in the United States, primarily due to deaths from chronic obstructive pulmonary disease (COPD).¹ COPD is defined as airflow limitation that is not fully reversible.² Airflow limitation in COPD results from structural changes in the airway wall, bronchoconstriction and lack of tethering due to emphysema.^{3–7}

Smoking is the major risk factor for COPD,^{8–11} and chronic smoking is associated with pigmented macrophages, edema, fibrosis and epithelial hyperplasia in first and second order respiratory bronchioles in autopsy specimens from healthy smokers.¹² Chronic smoking is associated with inflammatory infiltrates, fibrosis and squamous cell metaplasia in lung biopsy specimens.¹³

Two prior case-control studies examined the relationship between chronic smoking and airway dimensions on computed tomography (CT) scan.^{14,15} Both studies, however, used measures of airway dimensions that are a function of both wall thickness and lumen diameter. The first measure, airway wall area percent (WA%), is usually defined as the total airway area minus the lumen area divided by the total airway area.⁷ The second, Pi10, regresses the wall thickness on lumen diameter from all visualized airways to calculate the hypothetical airway wall thickness (AWT) of an airway at an internal perimeter of 10 mm.¹⁶ An increased WA% or Pi10 are usually interpreted as evidence of thicker airway walls^{17–19} but higher values of these measures could result mathematically from thicker walls, narrower lumens or a combination of the two. Hence, if acute and chronic cigarette smoke exposure differentially affect airway lumen diameter and AWT, the use of a combined measure such as Pi10 or WA% may not detect these differences.

In addition, the two existing case-control studies may be limited by selection bias due to differential selection of cases compared to controls, reverse-causality in which aspects of clinical COPD affect airway dimensions, or limited generalizability.

We therefore examined AWT and airway lumen diameter on CT scan in a large, population-based cohort study hypothesizing that cumulative smoking would be associated specifically with thicker airway walls in segmental bronchi. Given prior paradoxical findings of the association of emphysema on CT scan with current smoking,²⁰ we also examined the association of current smoking with AWT and airway lumen diameter.

Methods

Multi-Ethnic Study of Atherosclerosis

The Multi-Ethnic Study of Atherosclerosis (MESA) is a multi-center cohort study of subclinical cardiovascular disease in whites, African Americans, Hispanics, and Asians.²¹ Between 2000 and 2002, MESA recruited 6814 men and women 45–84 years of age from Forsyth County, North Carolina; New York City; Baltimore; St. Paul, Minnesota; Chicago; and Los Angeles. Exclusion criteria were clinical cardiovascular disease, weight exceeding 136 kg (300 lb.), pregnancy, and impediment to long-term participation.

The MESA Family Study recruited 1595 African American and Hispanic participants, generally siblings of MESA participants, using the same inclusion and exclusion criteria as MESA except that clinical cardiovascular disease was permitted (Fig. 1).²²

The MESA Air Pollution Study recruited an additional 257 participants from Los Angeles and Riverside County, CA, and Rockland County, NY, using the same criteria as MESA except that participants were ages 50–89 who lived in the area $\geq 50\%$ of the year and had no plans to move in the next five years.²³

MESA, MESA Family, and MESA Air Pollution studies used the same study protocol for the measures presented here.

The protocols were approved by the institutional review boards of all collaborating institutions and by the National Heart, Lung, and Blood Institute. All participants provided written informed consent.

Smoking status and pack years

Smoking status and pack years were assessed via standard American Thoracic Society questionnaire items²⁴:

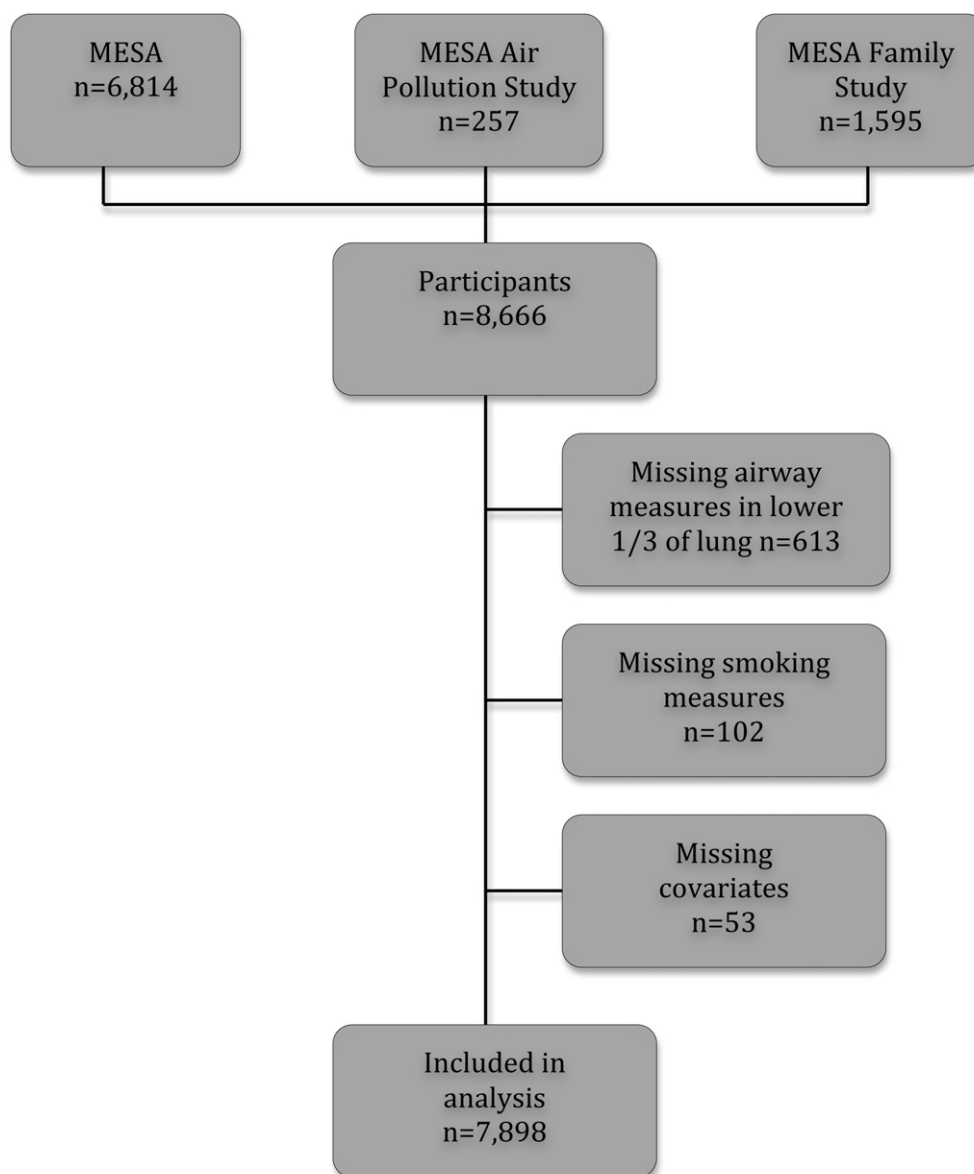


Figure 1 Participants in the Multi-Ethnic Study of Atherosclerosis (MESA) studies included in the analysis.

"Have you smoked at least 100 cigarettes in your lifetime?"

"How old were you when you first started smoking cigarettes?"

"Have you smoked during the last 30 days?"

"How old were you when you quit smoking cigarettes?"

"On average, about how many cigarettes a day do/did you smoke?"

Participants who reported smoking fewer than 100 cigarettes in their lifetimes were classified as never

smokers. Among participants who reported smoking greater than 100 cigarettes in their lifetime, those who reported smoking during the last 30 days were classified as current smokers and those who did not were classified as former smokers. Pack-years of cigarette smoking were calculated from age of starting to quitting (or current age among current smokers) \times (cigarettes per day/20). Urinary cotinine levels were measured via immunoassay in a subset of 3674 MESA participants (Immulite 2000 Nicotine Metabolite Assay; Diagnostic Products Corp., Los Angeles, CA).²⁵

CT measures

Lung structure was assessed on the lung fields of cardiac CT scans, which included approximately 70% of the lung volume from the carina to the lung bases. Cardiac CT scans were obtained at full inspiration on multidetector-row (MDCT) and electron-beam (EBT) CT scanners according to

a standardized protocol.²⁶ The scans were cardiac-gated, thereby reducing cardiac-related motion artifact in the left lower lobe. Two scans were obtained for each participant within the same session. The scan with the greater volume of lung air was used for analyses, except in cases of discordant scan quality, when the higher-quality scan was analyzed.²⁷

The CT scans were sent to a single center, the Iowa Comprehensive Lung Imaging Center, where the scans were read by nine radiology analysts using a modified version of the Pulmonary Analysis Software Suite (PASS)^{28,29} with semi-automated airway analysis.³⁰ PASS is a software package that enables the manipulation, display and analysis of multidimensional digital imaging data and was used in the NHLBI-funded National Emphysema Treatment Trial.³¹ The airway tree was identified and labeled, paths identified and straightened so as to provide luminal and wall dimensions measured as a function of the distance along the path and perpendicular to the local long axis (Fig. 2). All airways that were sampled by CT imaging approximately perpendicular to the airway long axis (i.e., the airway lumen was approximately circular) were measured in two dimensions using a modified full-width-half-maximum principal to identify the outer and inner airway wall borders.^{30,32–34} Earlier full-width-half-maximum methods gave inaccurate results for small thin-walled structures like airways. To address this problem,

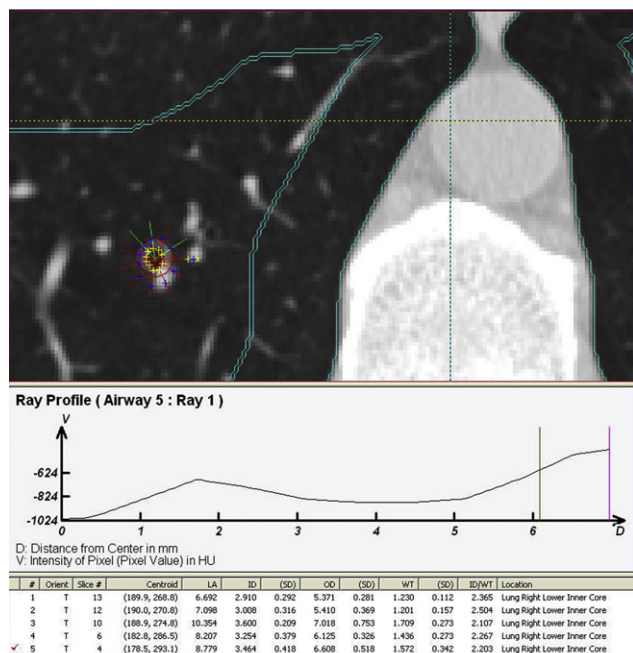


Figure 2 Airway measurements on CT scan. Upon locating an airway perpendicular to the plane, a centroid was placed in the center of the airway, from which the Pulmonary Analysis Software Suite generated rays and inner and outer airway diameters. If a ray extended into adjacent tissue the analyst would manually exclude it and the PASS system would regenerate the inner and outer diameter to better conform to the shape of the airway. The remaining rays were averaged to calculate airway wall thickness and lumen diameter.

PASS assessed the point-spread function of the particular scanner/slice selection/reconstruction algorithm of interest and then used a model-based deconvolution to account for the scanning process. This approach was more accurate than earlier methods for thin-walled structures.^{29,35,36} Upon locating an airway perpendicular to the plane, a centroid was placed in the center of the airway, from which the PASS system generated rays and inner and outer airway diameters. If a ray extended into adjacent tissue the analyst would manually exclude it and the PASS system would regenerate the inner and outer diameter to better conform to the shape of the airway. The remaining rays were averaged to calculate airway wall thickness and lumen diameter (Fig. 2). Readers underwent standardized training and were certified based upon achievement of less than 5% inter-reader and intra-reader variability on a set of training scans.

AWT and airway lumen diameter were measured on the same slice in the airway with the largest luminal diameter in the basilar 1/3 of the scan, the posterior basal segmental bronchi (LB10 or RB10). We validated this approach among 31 MESA participants who underwent concurrent full-lung CT scans and found that 95% of airways selected using this algorithm were either LB10 or RB10.

A total of nine readers read 7898 scans. Four of these readers read 85% of the scans ($n = 6727$; mean 1682 scans per reader). The mean difference in airway wall thickness (AWT) between readers was 0.09 mm. The intra-scan intraclass correlation coefficients (ICCs) were excellent for airway lumen and airway wall area percent (0.94 and 0.92, respectively) and good/very good for AWT (0.68) among 266 randomly selected scans read by the same reader twice (with an intervening 6-month interval). The intra-scan, inter-reader ICCs were slightly lower at 0.87, 0.82 and 0.55, respectively, among 330 randomly selected scans read by different readers. The intra-scan ICCs for lumen diameter and wall thickness did not vary appreciably by smoking category: 0.88 and 0.58 for never smokers, 0.91 and 0.53 for former smokers, and 0.84 and 0.62 for current smokers. This quantitative approach to the assessment of airway analysis was more reproducible than physician assessment of airway dimensions.³⁷

To facilitate comparisons with the literature, we also report AW% and Pi10. AW% in segmental airways was defined as:

$$\left\{ \left[\pi(\text{outer diameter}/2)^2 - \pi(\text{inner diameter}/2)^2 \right] / \left[\pi(\text{outer diameter}/2)^2 \right] \right\} \times 100.$$

Pi10 in the lower lobes was calculated following the standard method. Individual regression plots were created for each participant, plotting the square root of the wall area against the corresponding internal perimeter for each measured airway belonging to that participant. As is standard, airways with an internal perimeter ≤ 6 mm were excluded given the technical limitations of the CT scanners. The resulting regression line was used to calculate the standardized measure of airway wall thickness for a hypothetical airway with an internal perimeter of 10 mm (Pi10) for each participant.^{16,17}

Covariates

Age, gender, educational attainment, occupational exposure to dust and physician-diagnosed asthma were self-reported. Anthropometry was assessed as previously described.³⁸ Genetic ancestry was defined by principal components derived from approximately 1 million genome-wide SNPs (Affymetrix 6.0) in the current cohort.³⁹ Average level of ambient particulate matter smaller than 2.5 μm ($\text{PM}_{2.5}$) in the year prior to the CT scan was estimated from a temporal-spatial model as previously described.²³

Statistical analysis

The cohort was stratified by smoking status for descriptive purposes. Linear regression was employed to test the relationship between smoking and airway dimensions with generalized estimating equations to account for the correlation among related family members.⁴⁰ Initial models were adjusted for age, sex and the first three principle components of ancestry. We then additionally adjusted for the following potential confounders of education, height, weight, asthma history and $\text{PM}_{2.5}$, in addition to CT scanner type and tube current as precision variables. An additional analysis for pack years additionally adjusted for cigarettes smoked per day among current smokers. Interactions were tested in the full model with the -2 log likelihood test. The linearity of association of pack years and AWT was evaluated using plots generated with fully adjusted generalized additive models. The tests of the primary hypothesis, 95% confidence intervals, and *P*-values were estimated from linear regression models. Statistical significance was defined as two-tailed *P*-values < 0.05 . Analyses were performed using SAS 9.1 (SAS Institute, Cary, NC).

Results

The mean age of the 7898 participants at the time of the CT scan was 62 ± 10 years, 46% were male, and the self-reported race/ethnic distribution was 33% white, 33% African-American, 25% Hispanic and 9% Chinese-American.

Fifty-one percent were never smokers, 35% were past smokers (median pack years, 14, inter-quartile range 5–31) and 14% were current smokers (median pack years, 24, IQR 12–40). Current smokers were younger and more likely to be male and African-American, whereas former smokers were older and more likely to be male and white (Table 1). The airway dimensions listed in Table 1 are crude and not adjusted for important covariates related to body size such as age, gender, and race/ethnicity.

Cumulative smoking

Pack years of smoking were associated with thicker segmental airway walls in both minimal and fully adjusted models (Table 2 and Fig. 3). There was no evidence that the magnitude of this association with AWT varied by race/ethnicity (*p*-interaction = 0.40), gender (*p*-interaction = 0.11) or scanner type (*p*-interaction = 0.43). In contrast, there was no evidence for an association of

pack years with segmental airway lumen diameter (Table 2). Findings were similar after the exclusion of participants with clinically diagnosed emphysema (0.002 mm [-0.0001 to -0.004]; *p* = 0.06).

In secondary analyses, pack years were also associated with increased Pi10 (0.005 mm per 10 pack-years of smoking [95% CI 0.001, 0.009]; *p* = 0.008) and a consistent but non-significant increase in WA% (0.063% [95% CI -0.04 , 0.162]; *p* = 0.2).

Current smoking

Current smoking was associated with narrower airway lumens in both minimal and fully adjusted models (Table 3) and there was no evidence that the magnitude of this association varied by race/ethnicity (*p*-interaction = 0.49), gender (*p*-interaction = 0.68) or scanner type (*p*-interaction = 0.83). In contrast, current smoking was not associated with segmental AWT (Table 2). Findings were similar after the exclusion of participants with clinically diagnosed emphysema (-0.11 mm [-0.20 to -0.02]; *p* = 0.02).

In secondary analyses, current smoking was associated with increased airway WA% (1.0% [95% CI 0.3, 1.6]; *p* = 0.002) but not increased Pi10 (0.02 mm [-0.02 , 0.05]; *p* = 0.4) in fully adjusted models. Defining current smoking as cotinine level >500 ng/ml in the subset with cotinine measures (467 of 3674 participants) yielded qualitatively similar results: an association of current smoking with narrower airway lumens (-0.13 mm [95% CI -0.25 , 0.00018]; *p* = 0.05) and increased WA% (1.3% [95% CI 0.44, 2.11]; *p* = 0.003).

Sensitivity analyses

Associations were similar after additionally controlling for occupational exposure to dust among the 3701 participants with available measures: pack years were associated with thicker airway walls (0.002 mm [95% CI 0, 0.004]; *p* = 0.03) and current smoking with narrower lumens (-0.12 mm [95% CI -0.24 , 0.011]; *p* = 0.07). Results were similar when analyses were restricted to the four readers who read the majority (*n* = 6727) of the CT scans: in these analyses, pack years were associated with thicker airway walls (0.002 mm [95% CI 0.0001, 0.004]; *p* = 0.04) and current smoking with narrower lumens (-0.13 mm [95% CI -0.22 , -0.03]; *p* = 0.009).

Findings were similar when the (*n* = 84) participants with other lung diseases such as bronchiectasis, lung cancer, sarcoidosis or tuberculosis were excluded: pack years of smoking were associated with thicker airway walls (mean increase 0.002 per ten pack years [0.0002–0.0042]; *p* = 0.03) and current smoking was associated with narrower airway lumens (mean decrease -0.10 mm [-0.2 to -0.01]; *p* = 0.03) in fully adjusted models.

Findings also were qualitatively similar when analyses were stratified by scanner type. Every 10 pack years was associated with a 0.003 mm increase in AWT on MDCT scanners (95% CI 0.00029, 0.005; *p* = 0.03) and a 0.002 mm increase in AWT on EBT scanners (95% CI 0.000, 0.005; *p* = 0.3). Current smoking was associated with narrower

Table 1 Characteristics of the study sample stratified by smoking status.

<i>N</i> = 7898	Never smokers <i>N</i> = 3999	Former smokers <i>N</i> = 2796	Current smokers <i>N</i> = 1103
Age, mean (SD), years	62 (10)	63 (10)	58 (9)
Female gender – no. (%)	2521 (63)	1228 (44)	513 (47)
Race/ethnicity – no. (%)			
White	1148 (29)	1141 (41)	296 (27)
African American	1212 (30)	887 (32)	490 (44)
Hispanic	1078 (27)	622 (22)	276 (25)
Chinese	561 (14)	146 (5)	41 (4)
Principal components of ancestry (PC) – median (IQR)			
PC1	0.09 (0.03–0.61)	0.06 (0.02–0.58)	0.10 (0.02–0.77)
PC2	0.23 (0.04–0.35)	0.17 (0.03–0.27)	0.22 (0.04–0.28)
PC3	0.23 (0.17–0.26)	0.2 (0.17–0.26)	0.24 (0.18–0.27)
Pack years, median (IQR)	0 (0)	14 (4.63–31)	24 (11.7–40)
Education, years – no. (%)			
<12	813 (20)	425 (15)	209 (19)
12	715 (18)	475 (17)	224 (20)
>12	2471 (62)	1896 (68)	670 (61)
Asthma self report – no. (%)	393 (10)	295 (11)	100 (9)
Height, mean (SD), cm	164 (10)	168 (9)	169 (10)
Weight, mean (SD), lbs.	171 (38)	182 (38)	177 (39)
Occupational exposure to dust – no. (%) ^a	613 (32)	522 (39)	215 (47)
PM _{2.5} , mean (SD)	12 (8.4)	12 (7.7)	11 (8.2)
CT type – no. (%)			
Imatron	2124 (53)	1308 (47)	474 (43)
Volume zoom	907 (23)	780 (28)	312 (28)
Lightspeed plus	379 (9)	335 (12)	125 (11)
Sensation cardiac 64	168 (4)	107 (4)	30 (3)
Lightspeed Pro 16	142 (4)	77 (3)	44 (4)
Aquilion	120 (3)	59 (2)	51 (5)
Sensation 16	89 (2)	60 (2)	45 (4)
Lightspeed QX/i	70 (2)	70 (3)	22 (2)
Airway luminal diameter, mm, mean (SD)	3.32 (1.17)	3.43 (1.21)	3.21 (1.18)
Airway wall thickness, mm, mean (SD)	1.43 (0.19)	1.44 (0.19)	1.43 (0.19)
Airway wall area percent, %, mean (SD)	71.9 (8.03)	71.3 (8.15)	72.9 (8.12)
Airway Pi10 mm, mean (SD)	4.59 (0.54)	4.59 (0.34)	4.6 (0.55)

MESA = Multiethnic Study of Atherosclerosis, SD = standard deviation, IQR = inter-quartile range, PC = principal components, PM_{2.5} = ambient particulate matter smaller than 2.5 µm.

^a Among *n* = 3701 participants for whom data were available.

lumens on MDCT scanners (−0.08 mm [95% CI −0.18, 0.027]; *p* = 0.1) and EBT scanners (−0.16 mm [95% CI −0.27, −0.05]; *p* = 0.005). The exclusion of results from the Toshiba scanners yielded identical results for pack years and increased the significance of those for current smoking (−0.12 mm [95% CI −0.21, −0.03]; *p* = 0.009).

In order to assess for potential selection bias due to the exclusion for clinical cardiovascular disease, analyses were restricted to participants age less than 65 years. These analyses also yielded similar, significant results for pack years with AWT (0.003 mm [95% CI 0.00008, 0.006]; *p* = 0.01) and current smoking with airway lumens (−0.13 mm [95% CI −0.23, −0.03]; *p* = 0.01).

Discussion

Cumulative smoking was associated with thicker airway walls in this large, population-based cohort study. In

addition, current smoking was associated with narrowed airway lumens. This is by far the largest study of which we are aware to assess these measures and is unique in doing so in a general population sample.

Two prior case-control studies reported associations between smoking and Pi10. Patel et al. studied airway dimensions on CT scan in 519 smokers with COPD and 640 smokers (siblings of the cases), and reported an association between Pi10 and pack years (*r* = 0.26), although that study did not control for current smoking.¹⁵ Grydeland et al. studied 463 smokers with COPD and 431 smokers, and reported an association between pack years and Pi10, but only among controls.¹⁴ The present study replicated these prior results for Pi10 in a much larger, multi-ethnic, population-based cohort, which is less subject to selection bias.

Increases in the Pi10, however, may reflect an increase in AWT or a decrement in airway wall lumen and it is unclear which aspect contributed to the findings in the

Table 2 Mean differences in airway dimensions per ten pack years of cigarette smoking.

N = 7898	Per ten pack years	
	Mean difference (95% CI)	P-value
Airway wall thickness, mm		
Mean difference Model 1 ^a	0.004 (0.002–0.006)	0.0003
Mean difference Model 2 ^b	0.003 (0.0007–0.004)	0.008
Mean difference Model 3 ^c	0.002 (0.00002–0.004)	0.03
Airway lumen diameter, mm		
Mean difference Model 1 ^a	–0.01 (–0.02 to 0.008)	0.4
Mean difference Model 2 ^b	–0.01 (–0.02 to 0.002)	0.1
Mean difference Model 3 ^c	0 (–0.02 to 0.01)	0.7

Never-smokers were included in these analyses and coded as having zero pack years.

^a Model 1: age, gender, principal components of ancestry.
^b Model 2: Model 1 + education, height, weight, asthma, scanner type, CT voltage and PM_{2.5}.
^c Model 3: Model 2 + cigarettes per day among current smokers.

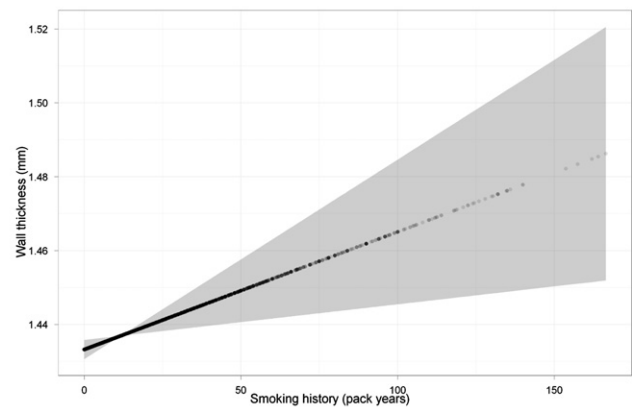
prior case-control studies. The present study addressed this gap using a novel approach to examine AWT separately from lumen diameter and demonstrated definitively that cumulative smoking is associated with increased AWT.

Changes in dimensions of segmental airways on CT scan are correlated with dimensions of the small conducting airways measured histologically¹⁶ and likely reflect airway remodeling, goblet cell hyperplasia or both. Increased mucus in the airway lumen is an alternative explanation as mucus is indistinguishable from wall on quantitative CT scanning; however, this is an unlikely explanation for the finding of increased AWT as cumulative smoking was not associated with reduced lumen diameter, as would be expected with mucus.

The mechanism of smoking-induced small airway remodeling in humans remains an open question. Chronic smoke exposure causes increased airway wall collagen in mouse^{41–43} and guinea pig models.⁴⁴ Guinea pigs exposed to cigarette smoke for six months had increased AWT and increased thick collagen fibers in airway walls, which were associated with reduced peak expiratory flow and FEV₁/FVC, and increased airway resistance.⁴⁵ Acute smoke exposure leads to upregulation of type I pro-collagen and transforming growth factor- β (TGF- β) gene expression in mice,⁴² and upregulation of collagen and TGF- β in rats.⁴⁶ In guinea pigs exposed to cigarette smoke, small airway remodeling was blocked by an inhibitor of matrix metalloproteinases 9 and 12.⁴⁴

Alternatively, higher levels of exposure to cigarette smoke were associated with more severe pathophysiologic changes in the small airways, including goblet cell metaplasia, and the severity of these changes was associated with decreased lung function in smokers undergoing

a Wall thickness



b Lumen diameter

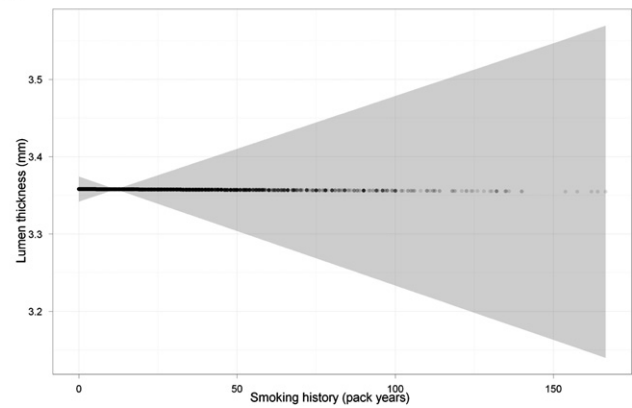


Figure 3 Continuous relationships of cigarette pack years to airway measures. (a) Wall thickness. (b) Lumen diameter. The plots show the smoothed association for airway dimensions per ten pack years for mean levels of other covariates from a multivariable generalized additive model using repeated measures assuming compound symmetric covariance within MESA family units. Never-smokers were coded as having zero pack years.

Table 3 Mean differences in airway dimensions among 1103 current smokers compared to never smokers.

	Mean difference (95% CI)	P-value
Airway wall thickness, mm		
Mean difference Model 1 ^a	0.008 (–0.01–0.02)	0.3
Mean difference Model 2 ^b	0.005 (–0.01–0.02)	0.5
Airway lumen diameter, mm		
Mean difference Model 1 ^a	–0.17 (–0.2 to –0.09)	<0.0001
Mean difference Model 2 ^b	–0.11 (–0.2 to –0.02)	0.02

The reference group is comprised of non-smokers. Findings for former smokers are reported in the text.

^a Model 1: age, gender, principal components of ancestry.
^b Model 2: Model 1 + education, height, weight, asthma, scanner type, CT voltage, PM_{2.5} and pack years.

resection for pulmonary tumors.⁴⁷ Several investigators have observed increased numbers of goblet cells in the small airways of smokers.^{7,48} Smoking-related increases in the number, size or function of goblet cells in the small airways might reduce lung function either via mucus plugs that completely occlude the airway lumen, or by altering airway surface tension.^{47,49}

We also observed that current smoking was associated with smaller airway lumens. Mucus may be one explanation for this finding, and greater WA% on CT scan previously has been associated with chronic bronchitis⁵⁰; however, current smoking was not associated with increased AWT, as would be expected with goblet cell hyperplasia and mucus secretion. Alternative explanations include bronchoconstricting effects of acute smoke exposure⁵¹ or of acute smoking-related inflammation.⁵²

The present study has a number of limitations. The magnitude of the increase in wall thickness observed in this study was modest. However, the study participants were recruited from the general population, so the increase related to smoking is expected to be smaller than that previously observed in clinical populations of patients with COPD. In addition, measurement error in AWT may have led to an underestimate of the true association, given that the measurement error was not related to smoking status and hence likely biased associations toward the null. Airflow in the small peripheral airways can be modeled using Poiseuille's Law, in which airflow is proportional to airway radius to the fourth power.⁴⁹ Thus, to the extent that airway dimensions in segmental airways predict dimensions in small peripheral airways, even the comparatively small differences in airway dimensions associated with smoking in this study may have important implications for airflow limitation. This is consistent with the findings of Hogg and colleagues, who observed relatively greater airway wall thickening in patients with early stage COPD and greater destruction of the small airways in participants with more advanced disease.⁵³

There is potential for misclassification of smoking history given its retrospective ascertainment. Current smoking may have been misrepresented; however, analysis based upon cotinine-confirmed smoking status in half the cohort yielded similar results. Furthermore, discrepancies of self-reported vs. cotinine-confirmed smoking were rare and non-differential by airway wall thickness, which suggests results for current smoking and possibly pack years are conservative.

Cross-sectional studies may be limited by selection bias, but such bias is unlikely to explain the results since the study was population-based, participants were not selected based on airway dimensions, and findings persisted when analyses were restricted to participants less than 65 years of age, a group relatively free of exclusions for cardiovascular disease.

Lung structure was measured on the lung regions of cardiac-gated CT scans. Two dimensional measures of airway wall thickness and lumen diameter were assessed using methods similar to those used by Aysola et al., whose CT airway measures correlated with airway epithelial thickness on endobronchial biopsy samples.⁵⁴ The cardiac scans did not allow assessment of upper-lobe airways; however it is unclear if lower or upper airway measures are

preferred and they are correlated.⁵⁴ The resolution of the scans was sufficient to measure segmental airways but not smaller airways that are arguably the more relevant site for investigation of smoking-related pathophysiology. Other investigators have shown that segmental airway thickening is correlated with thickening in the more distal small airways.¹⁶ The scans did not allow for three-dimensional reconstruction, which may affect external validity, but would not affect internal validity. Cardiac-gating reduced the motion artifact typical in the left lower lobe of full lung scans, allowing more precise measures in both lower lobes. Variations in slice thickness and scanner resolution by scanner type may have affected airway measurement accuracy. However, this variability existed across all subgroups, scanner type was accounted for within the statistical models, and findings were similar when analyses were stratified by scanner type. Finally, observational studies are potentially subject to confounding; however, smoking is the dominant risk factor for COPD and we adjusted for multiple potential confounders.

In conclusion, our findings suggest that chronic cigarette smoking, as measured by pack years, is associated with thicker airway walls, and that current smoking is associated with narrower airway lumens. Smoking likely contributes to changes in airway wall structure prior to the development of clinical disease.

Authors' contributions

Dr. Donohue performed the statistical analysis and drafted the manuscript. Drs. Hoffman, Guo, Budoff, Austin, and Ms. Baumhauer provided data collection and critical revisions. Drs. Kalhan, Kawut and Tracy provided critical revisions. Dr. Barr provided funding, data collection and critical revisions.

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Conflict of interest statement

Eric Hoffman and Junfeng Guo are share-holders in and Ms. Baumhauer was a paid consultant to VIDA Diagnostics, a company that is commercializing lung image analysis software developed, in part, at the University of Iowa.

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